

# Atypical face shape and genomic structural variants in epilepsy

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Many pathogenic structural variants of the human genome are known to cause facial dysmorphism. During the past decade, pathogenic structural variants have also been found to be an important class of genetic risk factor for epilepsy. In other fields, face shape has been assessed objectively using 3D stereophotogrammetry and dense surface models. We hypothesized that computer-based analysis of 3D face images would detect subtle facial abnormality in people with epilepsy who carry pathogenic structural variants as determined by chromosome microarray. In 118 children and adults attending three European epilepsy clinics, we used an objective measure called Face Shape Difference to show that those with pathogenic structural variants have a significantly more atypical face shape than those without such variants. This is true when analysing the whole face, or the periorbital region or the perinasal region alone. We then tested the predictive accuracy of our measure in a second group of 63 patients. Using a minimum threshold to detect face shape abnormalities with pathogenic structural variants, we found high sensitivity (4/5, 80% for whole face; 3/5, 60% for periorbital and perinasal regions) and specificity (45/58, 78% for whole face and perinasal regions; 40/58, 69% for periorbital region). We show that the results do not seem to be affected by facial injury, facial expression, intellectual disability, drug history or demographic differences. Finally, we use bioinformatics tools to explore relationships between facial shape and gene expression within the developing forebrain. Stereophotogrammetry and dense surface models are powerful, objective, non-contact methods of detecting relevant face shape abnormalities. We demonstrate that they are useful in identifying atypical face shape in adults or children with structural variants, and they may give insights into the molecular genetics of facial development.

**Keywords:** epilepsy; dysmorphism; structural variants; genomics; dense surface models

**Abbreviations:** FSD = face shape difference

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## Introduction

Human face shape is strongly influenced by genetic factors. Studies in twins, siblings and populations show significant heritability for craniofacial dimensions (Kohn, 1991; Martínez-Abadías *et al.*, 2009). Conversely, 30–40% of genetic disorders have craniofacial manifestations (Hart and Hart, 2009). Some of these disorders are caused by pathogenic genomic rearrangements or pathogenic structural variants that comprise duplications, deletions, inversions and translocations (Winter, 1996; Slavotinek, 2008). Many such syndromes have a characteristic facial 'gestalt' that is important in clinical genetic diagnosis and management (Hennekam *et al.*, 2010). Traditionally, karyotyping has been used to identify large structural variants.

The advent of next-generation sequencing and chromosome microarrays, comprising single nucleotide polymorphism genotyping or array comparative genomic hybridization, has allowed detection of smaller novel pathogenic structural variants (Alkan *et al.*, 2011), which are being increasingly recognized as an important contributor to neurological and psychiatric disorders, such as epilepsy. Collectively, pathogenic structural variants are currently the most common known genetic risk factor for epilepsy, being present in 4–5% of individuals with the condition (Sisodiya and Mefford, 2011). They are implicated in different types of epilepsy (de Kovel *et al.*, 2009; Dibbens *et al.*, 2009; Helbig *et al.*, 2009; Heinzen *et al.*, 2010; Striano *et al.*, 2012; Galizia *et al.*, 2012), including those previously ascribed to structural changes, such as hippocampal sclerosis (Catarino *et al.*, 2011). Individual pathogenic structural variants are also associated with a range of neurological, psychiatric and other illnesses (Girirajan and Eichler, 2010). For example, the 15q13.3 microdeletion has been linked with autism (Miller *et al.*, 2009), schizophrenia (Stefansson *et al.*, 2008), epilepsy (Helbig *et al.*, 2009) and intellectual disability with facial dysmorphism (Sharp *et al.*, 2008).

Identifying genomic changes improves clinical management. In a study of an adult clinical genetics service, a genetic or genomic diagnosis led to appropriate specialty referral, better symptom management, diagnosis-specific preventive care, prenatal and family testing, recurrence risk information and referral to support organizations (Maves *et al.*, 2007). In epilepsy, testing may end the 'diagnostic odyssey' and assist in management (Ottman *et al.*, 2010; Kasperavičiūtė *et al.*, 2011). However, although newer genetic techniques may sometimes reveal an underlying cause, the amount of data emerging from such newer methods, and the current comparative lack of control data, can make interpretation difficult, for example, which variant, if any, in an individual's genetic data set is relevant (Buysse *et al.*, 2009; Vermeesch *et al.*, 2011), and which may simply be irrelevant or a rare polymorphism? Additional phenotyping might assist in establishing the significance of detected variants (Hennekam and Biesecker, 2012).

Face shape analysis may be able to help identify people with underlying genetic abnormalities, including pathogenic structural variants, particularly in those with neurological and psychiatric disorders, and could, thus, also help in interpretation of genetic findings. The ready identification of Down syndrome by recognition of its facial gestalt is one familiar example. Embryologically, face and

forebrain precursors develop closely together and activate similar genetic pathways (Marcucio *et al.*, 2011). Neural crest cells, derived from neural ectoderm, are primarily responsible for facial morphogenesis and are dependent on signals from the developing forebrain (Cordero *et al.*, 2011). Clinically, disturbances of early craniofacial development are associated with brain abnormalities, in disorders such as cleft lip/palate or schizophrenia (Waddington *et al.*, 1999; Nopoulos *et al.*, 2002).

A powerful basis for investigating facial shape is 3D stereophotogrammetry, which allows for rapid, accurate, non-contact capture of face images, generating surfaces available for further analysis. The technique has been used in orthodontics (Lane and Harrell, 2008), forensic science (Evison *et al.*, 2010), dysmorphology (Hammond, 2007) and to study variation across ethnic groups (Kau *et al.*, 2010). Dense surface modelling is a statistical method that can be used to analyse surface images, for example, to discriminate between well-known genomic disorders, including Williams syndrome, Smith–Magenis syndrome, 22q11 deletion syndrome, Noonan syndrome, Fabry disease and Cornelia de Lange syndrome (Hammond *et al.*, 2005; Cox-Brinkman *et al.*, 2007). It has also been used to detect previously unrecognized facial dysmorphism in Bardet–Biedl syndrome, which is thought to be caused by defects in genetic pathways affecting neural crest cell migration (Tobin *et al.*, 2008). A similar morphometric approach using laser surface imaging has identified subtle facial abnormalities in individuals with schizophrenia and bipolar disorder (Hennessy *et al.*, 2007, 2010).

Pathogenic structural variants contributing to neurological and psychiatric diseases may also affect facial shape, either directly or by affecting brain structure or function. We hypothesized that, among people with epilepsy, dense surface models can distinguish between those who do or do not have pathogenic structural variants. We explored this using an objective measure of face shape variation, called face shape difference (FSD), in three different regions of the face. We used this measure to predict the presence or absence of pathogenic structural variants in a second group of people with epilepsy. We then investigated factors that underlie or contribute to facial shape and excluded a number of potential confounders. As changes in facial shape related to pathogenic structural variants may be subtle and missed by clinicians caring for people with neuropsychiatric conditions (Galizia *et al.*, 2012), adjuncts to diagnosis may be helpful.

## Subjects and methods

The study was approved by the relevant ethics committees or institutional review boards. Written informed consent was obtained from study participants or informed assent was obtained from parents in accordance with local requirements and national standards.

### Patients

Patients were recruited in two phases over a period of 2 years. In the first phase, a training cohort of children and adults was recruited at the National Hospital for Neurology and Neurosurgery (UK), Meyer Children's Hospital (Italy), Erasmus Hospital (Belgium) and University Hospital Gasthuisberg (Belgium). All adults had a diagnosis of epilepsy,

made or reviewed by an epileptologist. Children were recruited if they were being investigated for epilepsy or if they had a diagnosis of epilepsy by a paediatric neurologist. People with known Mendelian epilepsy disorders or known chromosome imbalances were excluded.

In the second phase, during the following year, a validation sample of individuals with epilepsy from the same institutions was analysed after image capture and chromosome microarray analysis. They were included in a second set of face shape models and were used to determine the accuracy of the technique. These images were analysed and landmarked with the operator blinded to the results of the chromosome microarray analysis. All were patients in whom chromosome microarray testing had been requested independently of this study.

All participants were white Europeans. Non-Europeans were excluded from analysis because of insufficient ethnically matched control subjects. Participants who were outside the age range to have sufficient age-matched control subjects for comparison (<2 years; >52 years for male subjects or >54 years for female subjects) were also excluded. Medical records were reviewed for further information. Brain MRI results were categorized as normal, normal with incidental findings or abnormal based on clinical reporting by an experienced neuroradiologist. Intellectual disability was determined from neuropsychology reports, full-scale or verbal intelligence quotient (IQ) scores and clinical documentation of level of functioning in daily activities (Salvador-Carulla *et al.*, 2011). Because of the difficulty of accurate retrospective assessment of intellectual disability, especially in cases without formal neuropsychometry, only the following three categories were used: normal/mild, moderate or severe/profound; applying the definitions used for the same terms in the *International Classification of Diseases*, 10th Revision (World Health Organization, 1992). For adults, the earliest available neuropsychometric and clinical records were used to minimize confounding from potential effects on intellectual performance of chronic epilepsy, medical and surgical treatments and neurodegeneration.

## Control subjects

All patients' face surfaces were compared with a group of control subjects' face surfaces to calculate FSD. All of the control subjects were also white Europeans. They were recruited as volunteers, unaffected relatives of patients or healthy infants attending a routine postnatal clinic, from the UCL Institute of Child Health (London, UK). Control subjects had no known syndrome, previous craniofacial surgery or trauma. Control subjects had not been tested using chromosome microarrays, but as pathogenic structural variants are individually rare even in populations enriched for them and even less common in healthy individuals (Helbig *et al.*, 2009; Itsara *et al.*, 2009; Heinzen *et al.*, 2010), it is unlikely that bias resulted from lack of screening in control subjects.

## Pathogenic structural variant detection

Patients were included if they had undergone array comparative genomic hybridization as part of research or clinical workup, or they had had genome-wide genotyping of single nucleotide polymorphisms. We collectively refer to these methods as 'chromosome microarrays' after Mefford *et al.* (2012).

Oligonucleotide array comparative genomic hybridization was performed using the Nimblegen 135 K microarray (Roche Nimblegen) or Agilent 44 K/60 K/75 K/105 K microarrays (Agilent Technologies) in an accredited clinical laboratory in accordance with manufacturer's instructions. Additional fluorescence *in situ* hybridization and/or

karyotyping were performed in some cases. The laboratory determined whether a detected structural variant was pathogenic by comparison with public and internal databases.

For some individuals, pathogenic structural variants were identified using genome-wide single nucleotide polymorphism data as previously published (Heinzen *et al.*, 2010): in brief, structural variants were deemed to be pathogenic if they were >1 Mb in size or if found in specific regions known to be associated with epilepsy.

We acknowledge that debate continues about methods for determining the clinical significance of structural variants (Vermeesch *et al.*, 2011). For our purposes here, one of the standardized methods aforementioned was used to determine if people had pathogenic structural variants. Our aim was not to discover pathogenic structural variants *per se*, but to determine the utility of face shape analysis with respect to these predetermined pathogenic structural variants. To investigate whether our arbitrary threshold of 1 Mb affected our results, we repeated the analysis using thresholds of 500 kb and 250 kb. Standard quality control measures were still applied as before (Heinzen *et al.*, 2010).

## Bioinformatic analysis

Gene content in pathogenic structural variants was determined using the University of California, Santa Cruz Genome Browser (<http://genome.ucsc.edu>, hg version 18), accessed through the Genetic Diseases/Gene Discovery interface (<http://gedi.ci.uchicago.edu/>). Gene expression levels in the human foetal forebrain were acquired from the Human Brain Transcriptome database (<http://hbatlas.org/>). We noted only the peak level of expression in the human forebrain, between 50 and 200 days gestation. Gene expression in the forebrain was noted to be present if signal intensity was >10 (log<sub>2</sub> scale), and the number of such genes within a given pathogenic structural variant was counted.

## Image capture

For all patients, 3D face images were captured with a commercial stereophotogrammetric device (Vectra CR 3D; Canfield Scientific). For control subjects, images were captured using the MU2 commercial camera (3dMD) and the Vectra CR 3D. There is no significant difference between face images captured on different stereophotogrammetric cameras (Weinberg *et al.*, 2006), and multiple cameras have been used in previous studies (Hammond *et al.*, 2005).

Face images were captured with the subjects seated, facing directly towards the camera and with the face and chin fully uncovered. A bright target was used to direct gaze, and up to three images were taken with the subject's face as close to a neutral expression as possible.

## Image review and landmarking

A physician (J.N.) reviewed all patient images for any visible acquired face deformity, and those patients were later excluded from the relevant face shape model(s) in a sensitivity analysis. One operator (K.C.), always blinded to genomic data, manually annotated each patient image with 22 facial landmarks, termed 'landmarking' (Supplementary Table 1). The chosen landmarks have been previously shown to be accurate and reproducible (Gwilliam *et al.*, 2006; Toma *et al.*, 2009). Control subject images were annotated previously by another operator (P.H.). We assessed intra- and inter-operator reproducibility in this study by randomly selecting 20 images, which were landmarked twice. Mean landmark error was <1.5 mm

(Supplementary Table 2), and intra-class correlation coefficients were 0.999–1.000. For further details, see Supplementary material.

## Dense surface modelling

Dense surface modelling, described previously (Hutton *et al.*, 2003; Hammond, 2007), uses custom in-house software (ShapeFind; UCL, London, UK) to create a 'dense surface model' of the face by co-registration of landmarked images and the interpolation of densely corresponded points (Supplementary Fig. 1). The resulting surfaces are described by a set of principal components that can collectively describe >99% of the shape variation (Supplementary Fig. 2). For further details, see Supplementary material.

The following three models were created from control subjects and the training cohort together: for the whole face (Face1), the periorbital region only (Eyes1) or the perinasal region only (Nose1), using pre-existing templates (Fig. 1; Hammond *et al.*, 2005). Three further models (Face2, Eyes2, Nose2) were generated subsequently by addition of the validation cohort to the original control subjects and the training cohort. In this second model set, only the validation cohort was used to retest the FSD threshold.

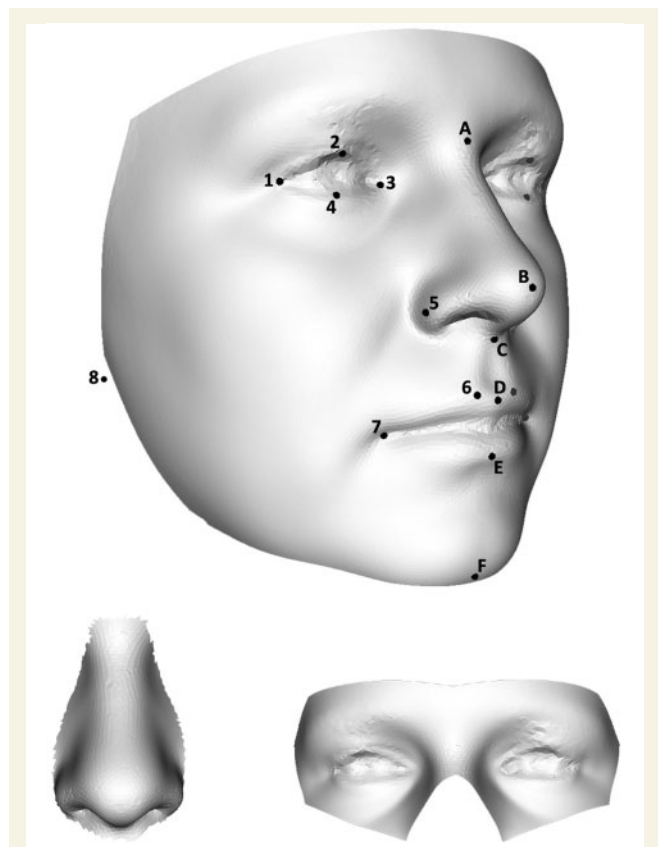
## Face shape difference

We matched every patient to the 30 closest sex-matched control subjects by age using contiguous running means. We then calculated the distance between each face and its matched mean control face in terms of the square root of the sum of squared differences of the respective principal components. This was called FSD and can be expressed algebraically as follows:

$$\text{FSD}(x,m) = \sqrt{\sum_{i=1}^n (x_i - m_i)^2} \text{ for } x \in M$$

where  $i$  indexes the  $n$  principal components capturing 99% shape variation in dense surface model  $M$ ,  $x$  is an arbitrary face and  $m$  is its matched mean in  $M$ . FSD provides a simple measure of the difference in face shape between a patient and their matched control mean in the model. An FSD value is not an absolute measurement: a given FSD value is always  $\geq 0$ , and it can only be compared with FSD values for other faces in the same model, because it is dependent on the underlying model whose principal components in turn reflect the faces analysed. FSD is measured in arbitrary units, and there are no predetermined values or thresholds for 'normal' shape. Principal components and FSD have been used previously (Hammond *et al.*, 2004, 2008).

The validity of FSD as a predictor of an underlying pathogenic structural variant was tested in the second cohort as follows: first, we demonstrated a linear relationship with strong positive correlation between FSD values in corresponding models of the same region of the face but with different composition of subjects (Face1 to Face2, Eyes1 to Eyes2 and Nose1 to Nose2). Then we used simple linear regression using least squares to quantify the exact relationship between FSD values in the corresponding models. Finally, we determined FSD threshold values with a chosen sensitivity and specificity in each of the original models (Face1, Eyes1, Nose1) and converted the values into equivalent inferred FSD threshold values in the second set of models (Face2, Eyes2, Nose2). These threshold values were then used to predict the presence or absence of pathogenic structural variants in the validation cohort. We then tested the prediction against laboratory results for presence or absence of pathogenic structural variants.



**Figure 1** Dense surface models of the face. Three regions of the face were used as base meshes to restrict the extent of the models. The upper image is also annotated with the landmarks used in model construction. The perinasal and periorbital regions are shown on the bottom left and bottom right, respectively. Landmarks A–F are in the midline. Landmarks 1–8 are paired and only shown for the right side of the face. They are as follows: A = nasion; B = pronasale; C = subnasale; D = labiale superius; E = labiale inferius; F = gnathion; 1 = exocanthion; 2 = palpebrale superius; 3 = endocanthion; 4 = palpebrale inferius; 5 = ala nasi; 6 = christa philtri; 7 = cheilion; 8 = lower auricular attachment. Landmark 8 is applied to all unprocessed face surface images, but the ears are omitted from the base mesh because of variable loss of surface at the image periphery because of occluding hair.

## Statistical methods

As the data were not normally distributed, we used the Mann-Whitney test with the null hypothesis that, in people with epilepsy, FSD was not different between those with pathogenic structural variants and those without pathogenic structural variants for the face, periorbital or perinasal areas. For data on ethnicity and intellectual disability, with >2 categories, the Kruskal–Wallis test was used. A receiver operating characteristic curve was calculated to assess sensitivity and specificity of the models. Fisher's exact test was performed for differences in categorical data. For correlation, the intra-class correlation coefficient was used to compare repeated measurements and Spearman's rank correlation coefficient for other data (weak correlation if  $0.25 \leq \rho < 0.5$ , moderate if  $0.5 \leq \rho < 0.75$ , strong if  $0.75 \leq \rho < 0.90$ , very strong if  $0.90 \leq \rho < 1.00$ ). A  $P$ -value  $< 0.05$

was considered significant. Bonferroni correction was applied for multiple comparisons. Analysis was conducted using SPSS version 20 software (SPSS Inc.).

## Results

### Subject population

The training cohort consisted of 148 individuals with epilepsy. Twenty-four were excluded due to lack of sufficient age-matched control subjects, and a further six were excluded because of lack of ethnically matched control subjects for comparison (Table 1), leaving 118 patients. Of these, 74 (63%) underwent genome-wide single nucleotide polymorphism array, with the remainder undergoing array comparative genomic hybridization with or without fluorescent *in situ* hybridization/karyotyping. Thirty-eight patients had pathogenic structural variants; this subset was compared with the remaining 80 without pathogenic structural variants. Those with pathogenic structural variants were younger, but age-matching accounts for this in all analyses. To create the models and calculate FSD, we added the face surfaces of 388 control subjects.

### Face shape difference in the training cohort

For each of the three models (Face1, Eyes1, Nose1), we calculated FSD for every patient. Those with pathogenic structural variants were then compared with those without pathogenic structural variants. The median FSD was significantly greater in those with pathogenic structural variants (Fig. 2A) than those without for all measures (whole face: 8.86 versus 7.65;  $P = 0.001$ , periorbital region: 10.6 versus 9.60;  $P = 0.013$ , perinasal region: 7.62 versus 7.01;  $P = 0.031$ , for pathogenic structural variant versus no pathogenic structural variant, respectively).

The distribution of FSD values reveals outliers for all models, in those with and those without pathogenic structural variants (Fig. 2A). FSD was still significantly greater in those with pathogenic structural variants after exclusion of all outliers (whole face:  $P = 0.001$ , periorbital region:  $P = 0.018$ , perinasal region:  $P = 0.018$ ).

FSD of the whole face shows a strong positive correlation with the periorbital region ( $\rho = 0.78$ ;  $P < 0.001$ ). The perinasal region is less strongly correlated with FSD in other facial regions ( $\rho = 0.50$ ;  $P < 0.001$  with whole face,  $\rho = 0.60$ ;  $P < 0.001$  with periorbital region).

### Face shape difference in the validation cohort

To substantiate the validity of FSD as a reflection of an underlying pathogenic structural variant in individual subjects, we tested how useful the models would be at an individual level. We created receiver operating characteristic curves (Fig. 2B). The area under the curve was 0.69 [95% confidence interval (CI) 0.60–0.80;  $P < 0.001$ ] for the Face1 model. An FSD value of 8.47 was the

optimal threshold for equal sensitivity and specificity (65.8%) in categorizing an individual face surface as one from a subject with a pathogenic structural variant. FSD threshold values were found for the Eyes1 and Nose1 models using the same approach (Table 2).

In the 81-subject validation cohort, 63 were analysed and 18 were excluded due to lack of matched control subjects. All these individuals had also undergone chromosome microarray testing for pathogenic structural variants (81% by genome-wide single nucleotide polymorphism array; 19% by array comparative genomic hybridization). For our training cohort, FSD values in the original and second (including the 63 patients) set of models showed strong positive correlation (Face1 versus Face2:  $\rho = 0.96$ ;  $P < 0.001$ , Eyes1 versus Eyes2:  $\rho = 0.96$ ;  $P < 0.001$ , Nose1 versus Nose2:  $\rho = 0.93$ ;  $P < 0.001$ ;  $n = 118$  for all), and a linear relationship was demonstrated (Fig. 2C).

In the validation cohort, the inferred whole face FSD threshold value (FSD = 9.99) correctly identified that 4 of 63 patients had pathogenic structural variants. One additional patient was also found to have a pathogenic structural variant (i.e. 4/5, 80% sensitivity). Similarly, whole face FSD correctly predicted that 45 patients had no pathogenic structural variants (45/58, 78% specificity). Using periorbital and perinasal FSD resulted in reduced sensitivity (3/5, 60% for both) and similar specificity (40/58, 69% and 45/58, 78%, respectively). Results are shown in Table 2.

### Exploration of face shape in patients with pathogenic structural variants

We next looked at whether there were any shared facial features in people with epilepsy and pathogenic structural variants. Given the diversity of pathogenic structural variants, we did not expect to find any common features. We examined every principal component for each patient's face surface and looked for any significant difference between those with and without pathogenic structural variants, using Bonferroni correction for multiple testing. Each principal component delineates a particular variation in face shape (Supplementary Fig. 2), and it can reflect a shared facial feature. No individual principal components were significantly different in those with pathogenic structural variants and those without in any of the models. There was also little difference between the average face of patients with pathogenic structural variants and the average face of those without pathogenic structural variants (Supplementary Fig. 3). Thus, we found no evidence for shared facial features across pathogenic structural variants.

### Genomic and clinical findings

We used the three models incorporating the training and validation cohort (Face2, Eyes2, Nose2) to explore the genomic and clinical data.

Exact breakpoints of the pathogenic structural variants were known for 39 patients (Supplementary Table 4). Four others with pathogenic structural variants had translocations or inversions detected by fluorescent *in situ* hybridization or karyotyping, and so full data on pathogenic structural variant size were not available. There was no correlation between whole face FSD and the

**Table 1** Subject recruitment

Variable or measure	Patients with pathogenic structural variants	Patients without pathogenic structural variants	Control subjects
Training cohort	42	106	NA
Excluded because of age; <i>n</i> (%)	2 (4.8)	22 (20.8)	–
Excluded because of ethnicity; <i>n</i> (%)	2 (4.8)	4 (3.7)	–
Number included; <i>n</i> (%)	38 (90.4)	80 (75.5)	–
Validation cohort	6	75	NA
Excluded because of age; <i>n</i> (%)	0	11 (14.7)	–
Excluded because of ethnicity; <i>n</i> (%)	1 (16.7)	6 (8.0)	–
Number included; <i>n</i> (%)	5 (83.3)	58 (77.3)	–
Total number included in study	43	138	388
Age; mean age, years (range)	25.8 (3.3–53.9)	38.8 (2.8–56.3)	21.3 (2.4–53.2)
Adults aged > 18 years; <i>n</i> (%)	29 (67)	135 (98)	207 (53)
Male subjects; <i>n</i> (%)	23 (53)	54 (39)	196 (51)
MRI findings; <i>n</i> (%)			
Normal	16 (37)	51 (37)	
Incidental findings	2 (5)	8 (6)	
Abnormal	19 (44)	75 (54)	
Not performed/unavailable	6 (14)	4 (3)	
Intellectual disability; <i>n</i> (%)			
Normal/mild	22 (51)	131 (95)	
Moderate	7 (16)	4 (3)	
Severe/profound	12 (28)	3 (2)	
Unknown	2 (5)	0	
Detection method; <i>n</i> (%)			
Array CGH	31 (72)	21 (15)	–
SNP array	8 (19)	117 (85)	–
FISH/karyotyping	4 (9)	0	
Centre; <i>n</i> (%)			
London	19 (44)	135 (98)	388 (100)
Brussels/Leuven	6 (14)	–	–
Florence	18 (42)	3 (2)	–

Summary of all subjects who were recruited for 3D stereophotogrammetry, the number of subjects excluded and the number of subjects used in dense surface models. In the group with pathogenic structural variants, children were included, there were more male subjects, and subjects were recruited from three different centres. All patients were matched to control subjects based on age and sex for further analysis. MRI findings, intellectual disability and detection methods were obtained from clinical records and investigation reports.

CGH = comparative genomic hybridization; FISH = fluorescent *in situ* hybridization; NA = not applicable; SNP = single nucleotide polymorphism.

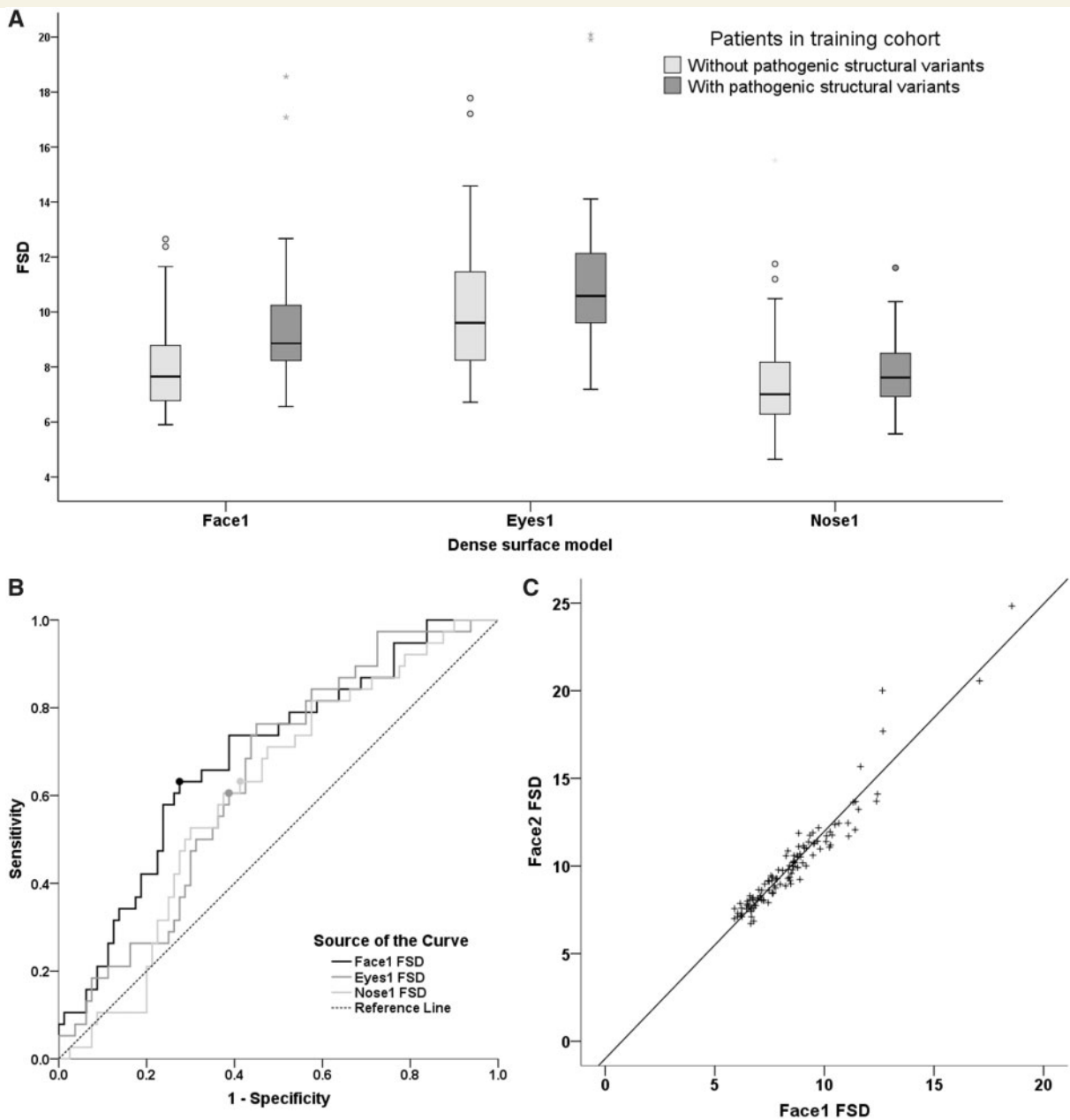
size of the pathogenic structural variant in terms of number of base pairs in the interval ( $\rho = 0.20$ ;  $P = 0.22$ ) or number of genes contained ( $\rho = 0.19$ ;  $P = 0.25$ ; Fig. 3A). Periorbital FSD showed weak correlation with the number of genes contained ( $\rho = 0.38$ ;  $P = 0.018$ ), but not the number of bases ( $\rho = 0.25$ ;  $P = 0.13$ ).

Within each pathogenic structural variant, we assessed the number of genes that were highly expressed in the human fetal forebrain (at 50–200 days gestation). Considering all participants with known pathogenic structural variant breakpoints, there was a weak positive correlation between the number of genes highly expressed in prenatal forebrain and whole face FSD ( $\rho = 0.34$ ;  $P = 0.036$ ;  $n = 39$ ; Fig. 3B). We looked at patients with deletions and duplications separately and excluded two patients with both types of pathogenic structural variants. A greater correlation coefficient was seen in patients with deletions ( $\rho = 0.36$ ;  $P = 0.07$ ;  $n = 26$ ) than in those with duplications ( $\rho = 0.15$ ;  $P = 0.67$ ;  $n = 11$ ), but this was not significant. Mean pathogenic structural

variant size and gene content were larger in patients with duplications than with deletions (11.5 Mb versus 2.48 Mb;  $P = 0.009$ , 49 genes versus 13.5 genes;  $P = 0.002$ ) as expected (Hanemaaijer et al., 2012), but mean FSD was not significantly different for all three models.

Brain MRI results were available for 171 of 181 patients, of which 67 were normal, 94 were abnormal and 10 were reported as normal with incidental findings (Table 1). Incidental findings comprised mild cortical atrophy, non-specific white matter lesions and in one case a cyst. There was no significant difference in class of MRI findings between the groups with and without pathogenic structural variants (Fisher's exact test;  $P = 0.71$ ). Patients with MRI abnormalities had a significantly greater FSD of the whole face than those with normal MRI findings (9.58 versus 8.81;  $P = 0.039$ ), but this was not true for the periorbital and perinasal models.

Intellectual disability was classified in our study population on the basis of formal neuropsychometry assessment in 127 subjects



**Figure 2** FSD in the training cohort. (A) Box plots of the median, interquartile range and range of FSD for the three different models using the training cohort ( $n = 118$ ). FSD is significantly greater for the whole face model (Face1: 8.86 versus 7.65;  $P = 0.001$ ), the periorbital model (Eyes1: 10.6 versus 9.60;  $P = 0.013$ ) and the perinasal model (Nose1: 7.62 versus 7.01;  $P = 0.031$ ) in patients with pathogenic structural variants. Outliers  $> 1.5$  or 3 times the interquartile range from the upper quartile are shown in circles or asterisks, respectively. Excluding all outliers does not alter significance. (B) Receiver operating characteristic curves of face FSD, periorbital FSD and perinasal FSD used for detecting pathogenic structural variants in the training cohort. The areas under the curve are 0.69, 0.64 and 0.61, respectively. The filled circles mark the optimal FSD threshold for equal sensitivity and specificity, used for prediction in the validation cohort in the second set of models (Face2, Eyes2, Nose2). (C) For the training cohort, there was very strongly positive correlation for FSD between the Face1 and Face2 models ( $\rho = 0.96$ ;  $P < 0.001$ ). This was also true for the periorbital and perinasal region (not shown; Eyes1 versus Eyes2:  $\rho = 0.96$ ;  $P < 0.001$ , Nose1 versus Nose2:  $\rho = 0.93$ ;  $P < 0.001$ ). Best-fit linear regression lines were used to convert the optimal FSD threshold values from the original model to the corresponding second model so that it could be used to predict the presence of pathogenic structural variants in the validation cohort. The formula for the line above is:  $\text{Face2 FSD} = (1.30 \times \text{Face1 FSD}) - 0.99$ .

**Table 2** Predictive accuracy of different dense surface models

Face region	Whole face	Periorbital region	Perinasal region
First models	Face1	Eyes1	Nose1
Number in training cohort	118	118	118
Area under the curve	0.69	0.64	0.61
Cut-off value	8.47	10.22	7.39
Predicted sensitivity	66% (25/38)	61% (23/38)	63% (24/38)
Predicted specificity	65% (52/80)	61% (49/80)	63% (50/80)
Second models	Face2	Eyes2	Nose2
Number in validation cohort	63	63	63
Equivalent cut-off value	9.99	12.96	8.66
Actual sensitivity	80% (4/5)	60% (3/5)	60% (3/5)
Actual specificity	78% (45/58)	69% (40/58)	78% (45/58)
Positive predictive value	26% (4/17)	14% (3/21)	19% (3/16)
Negative predictive value	98% (45/46)	95% (40/42)	96% (45/47)

Accuracy of models of the three different facial regions in identifying the presence of pathogenic structural variants in our validation cohort. The first set of models was created using the training cohort only, and from this, receiver operating characteristic curves were calculated, and an optimal cut-off value of FSD was chosen for equal sensitivity and specificity. An equivalent FSD threshold was used in the second set of models to predict the presence or absence of pathogenic structural variants in 63 new patients (see text for details). Prediction was most accurate using the whole face, in which measured sensitivity was 80% and specificity was 78%. The periorbital and perinasal regions are less sensitive and less specific.

and clinical records alone in a further 52 individuals. Two patients could not be categorized. There were significantly more people with moderate or severe/profound intellectual disability in the group with pathogenic structural variants. For all three regions of the face, FSD was significantly greater with increasing intellectual disability (Fig. 3C). For those who underwent formal neuropsychometric estimation of IQ, there was also a significant, but weakly negative, correlation between IQ score and FSD ( $\rho = -0.31$ ;  $P = 0.001$ ;  $n = 122$ ). We conducted a sensitivity analysis of only people with normal intellectual function or mild intellectual disability and found that FSD was still greater in people with pathogenic structural variants (whole face:  $P = 0.009$ , periorbital region:  $P = 0.048$ , perinasal region:  $P = 0.004$ ).

## Sensitivity analyses

### Ethnicity and age

We looked for any confounding factors in the combined patient cohorts using a series of sensitivity analyses, which are summarized in Supplementary Table 3. We found no significant difference in FSD due to age or ethnicity, noting our study population comprised children and adults from Belgium, Italy and UK (Supplementary material).

### Method of structural variant detection

The following three methods of analysis for pathogenic structural variants were used in this study: single nucleotide polymorphism arrays, array comparative genomic hybridization and fluorescent *in situ* hybridization/karyotyping in four of the subjects who also had array comparative genomic hybridization. Single nucleotide polymorphism arrays typically have poorer coverage of regions with structural variants than array comparative genomic hybridization (Cooper et al., 2008; Alkan et al., 2011). In our study, 72% of patients with pathogenic structural variants underwent array

comparative genomic hybridization, in contrast with only 15% of patients without pathogenic structural variants. We analysed only the people who underwent array comparative genomic hybridization ( $n = 52$ ) and still found a significantly greater median FSD in those with pathogenic structural variants, using the whole face model (11.1 versus 9.26;  $P = 0.005$ ; Fig. 3D) or the periorbital region (13.7 versus 12.0;  $P = 0.03$ ), but not the perinasal region (9.11 versus 8.21;  $P = 0.27$ ). This suggests the use of single nucleotide polymorphism array data is not necessarily a significant bias.

### Threshold of structural variant size used to determine pathogenicity

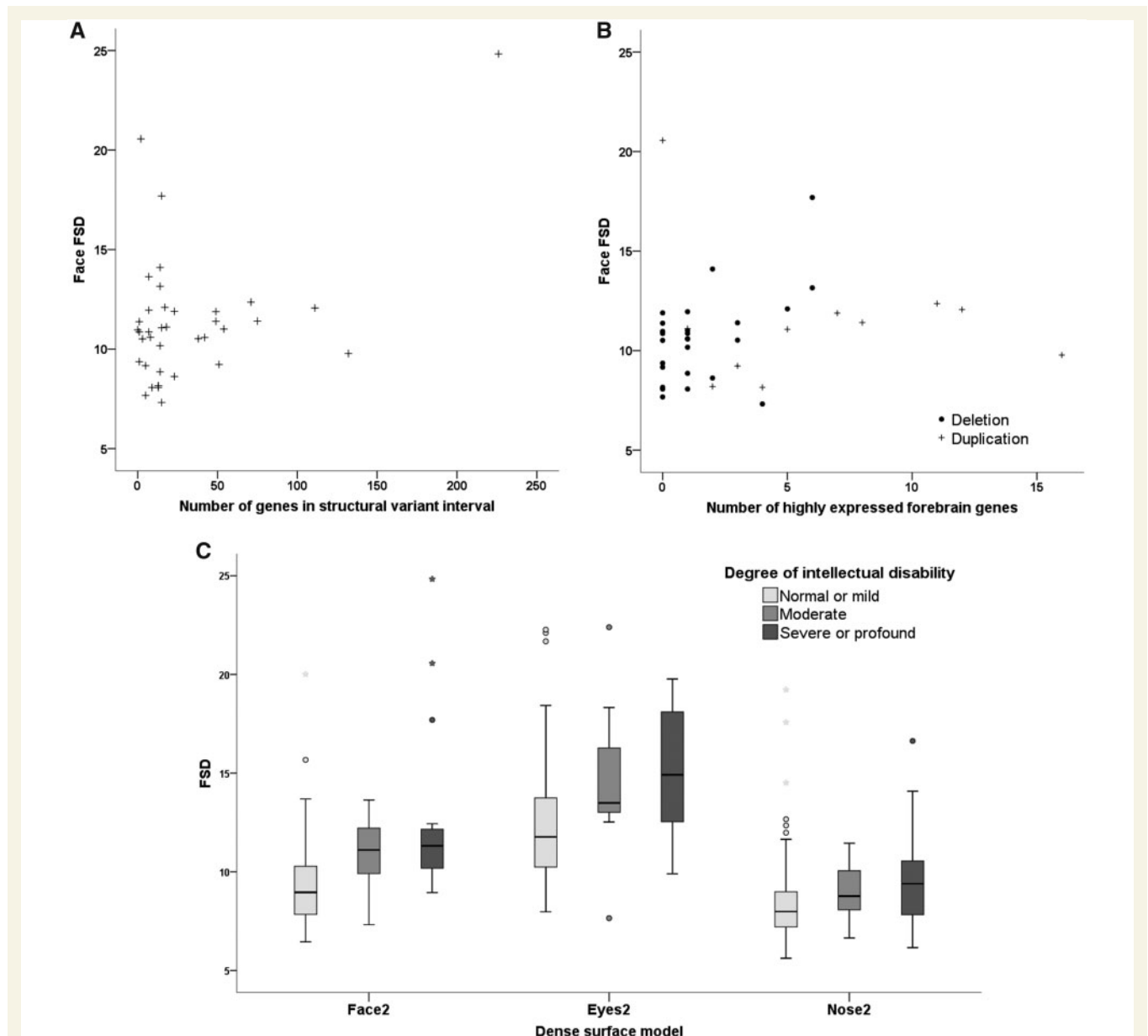
We had used a threshold of 1Mb as the lower limit for determining pathogenic structural variants from single nucleotide polymorphism array data (Heinzen et al., 2010), because there may be an increasing chance of 'false positive' calling of pathogenic structural variants with small threshold sizes (Itsara et al., 2009). We explored whether FSD was still significantly different for patients with structural variants if the lower limit for pathogenicity was set at 500 kb instead of 1Mb. At this threshold, three patients who had undergone single nucleotide polymorphism array were reclassified as having pathogenic structural variants. Repeat analysis showed that FSD remained significantly greater in patients with pathogenic structural variants ( $n = 46$ ) for the whole face (10.9 versus 8.87;  $P < 0.001$ ), the periorbital region (13.4 versus 11.4;  $P < 0.001$ ) and the perinasal region (8.91 versus 7.93;  $P = 0.001$ ). A further repeat analysis was conducted with the structural variant threshold size set at 250 kb, and now a further set of eight patients were reclassified with pathogenic structural variants ( $n = 54$ ), with no loss of significance for any of the models (whole face:  $P < 0.001$ , periorbital region:  $P = 0.002$ , perinasal region:  $P = 0.003$ ).



### Facial injuries and facial expression

A clinician (J.N.) reviewed all unprocessed 3D face images, blinded to all clinical details, and then excluded patients with probable acquired facial deformity. There was no significant difference in the number of images, thus, excluded between those with pathogenic structural variants and those without pathogenic structural

variants (Fisher's exact test; whole face,  $P=0.19$ ; periorbital region,  $P=1.0$ , perinasal region,  $P=0.12$ ). For the whole face model, 35 images were excluded. FSD was still significantly greater in people with pathogenic structural variants (10.9 versus 8.67;  $P < 0.001$ ). This was also true for the periorbital model after 15 exclusions (13.4 versus 11.2;  $P < 0.001$ ) and the perinasal model



**Figure 3** Analysis of face FSD with structural variant interval, intellectual disability and age in all patients. (A) There was no significant correlation between whole face FSD and the number of genes in the pathogenic structural variant interval ( $\rho = 0.19$ ;  $P = 0.25$ ), within all patients with available data ( $n = 39$ ). (B) Within the same group of patients, we identified genes in the structural variant interval that were highly expressed in the foetal forebrain. The number of such genes was correlated to whole face FSD ( $\rho = 0.34$ ;  $P = 0.036$ ;  $n = 39$ ), but when looking at those with deletions and those with duplications separately, there was no significant difference. (C) FSDs for the whole face, periorbital region or perinasal region were all significantly greater with increasing intellectual disability ( $P < 0.001$ ,  $P < 0.001$ ,  $P = 0.026$ , respectively;  $n = 179$ ). (D) We also assessed patients only undergoing array comparative genomic hybridization to exclude bias from different techniques to detect pathogenic structural variants, and found the median face FSD was still significantly different (11.1 versus 9.26;  $P = 0.005$ ;  $n = 52$ ). (E) Although patients with pathogenic structural variants were younger than those without pathogenic structural variants, no correlation was seen with age and whole face FSD.

(continued)

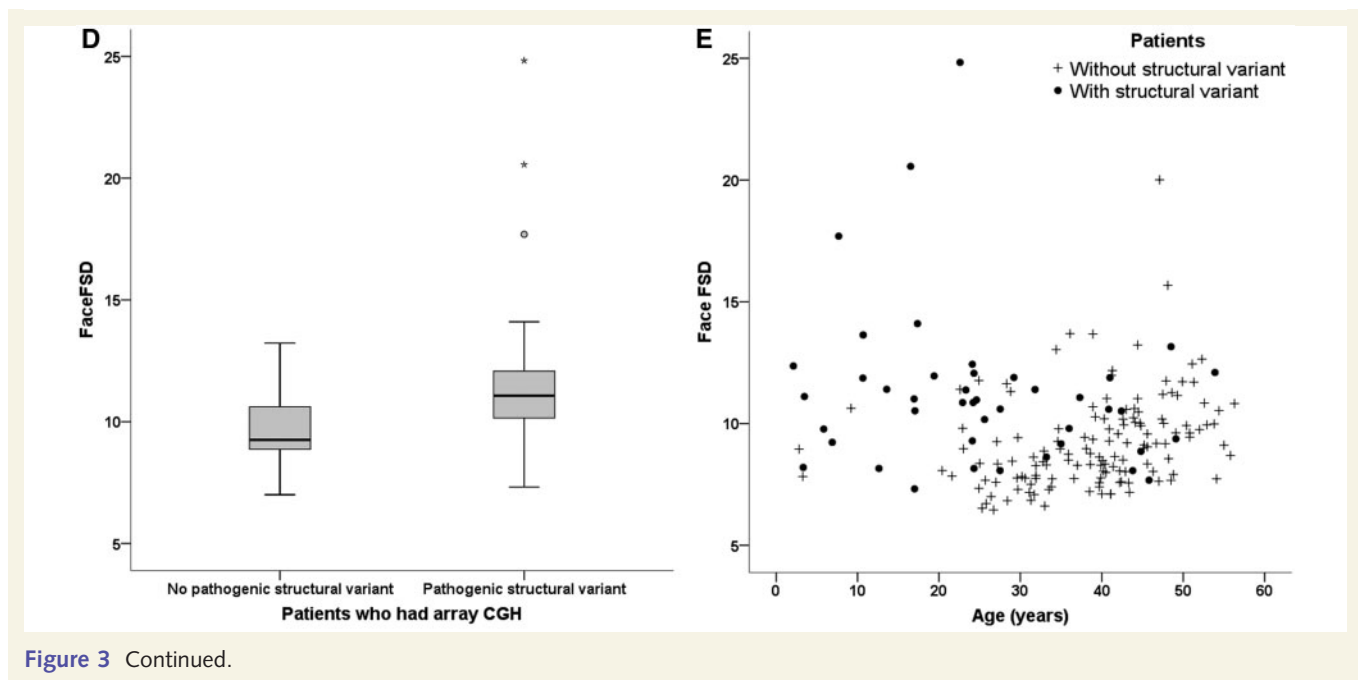


Figure 3 Continued.

after 10 exclusions (8.99 versus 7.87;  $P < 0.001$ ). Facial expression was also analysed, and this too was not a confounder in our study (Supplementary material).

### Anti-epileptic drug history

We assessed the effect of previous or current anti-epileptic drugs, because some are known to affect facial appearance after long-term use. Drug history was available for 170 of 181 patients (Supplementary Table 5). We compared adults with pathogenic structural variants to adults without pathogenic structural variants and found no significant difference in the number of anti-epileptic drugs used (six versus six;  $n = 158$ ;  $P = 0.12$ ). There was no significant difference between the number of adults with pathogenic structural variants who had used any given anti-epileptic drug and the number of those without pathogenic structural variants who had used it.

## Discussion

The findings support the hypothesis that for people with epilepsy, those with pathogenic structural variants have an objectively more atypical face shape compared with those without. This was true when analysing the whole face or just two feature-rich parts of the face, the periorbital region and perinasal region. Our technique had a sensitivity of 60–80%, specificity of 69–78%, positive predictive value of 14–26% and negative predictive value of 95–98% in an independent validation sample of people with epilepsy, although only five individuals had pathogenic structural variants in this sample. These findings were not explained by age, ethnicity, facial injury, facial expression, anti-epileptic drug history or the technique used to detect pathogenic structural variants, including structural variant threshold size. Our method comprised

computer-based facial shape analysis based on dense surface modelling. To our knowledge, this is the first time that dense surface modelling has been shown to discriminate, to a degree, between people with epilepsy with (different) pathogenic structural variants and those without pathogenic structural variants.

Of the three models, the whole face model is best at discriminating atypical facial shape at individual level, in the receiver operating characteristic curve analysis, and at group level, with a higher median FSD. This is in keeping with previous findings comparing the whole face with periorbital and perinasal regions in four known clinical syndromes (Hammond *et al.*, 2005). With an appropriate threshold, the expected and actual sensitivity and specificity of whole face FSD were 66–80% in detecting pathogenic structural variants. These findings were in spite of the heterogeneous nature of the group, comprising children and adults from three different European centres with different types of epilepsy and different pathogenic structural variants. Indeed, 31 of 43 patients have pathogenic structural variants that do not overlap with any others. Greater discrimination could be expected in more homogeneous groupings (Hammond *et al.*, 2005) and may emerge as more people with particular pathogenic structural variants are identified. We had only five patients with a recurrent pathogenic structural variant (16p13.11 deletion); no similarity was found in their face shape.

Evaluation for dysmorphism should be part of the clinical examination in epilepsy. Dysmorphism may be missed by untrained clinicians, and even clinical geneticists may take years to learn to recognize some patterns of facial dysmorphism (Reardon and Donnai, 2007). FSD is a quantitative analytical construct that can identify novel patterns of abnormality of facial anatomy. FSD changes identified in this study do not directly translate to clinically observable dysmorphism. Indeed, some of the study participants with high FSD values were not thought to be dysmorphic

when evaluated by their regular physician. We also found no difference for individual principal components in patients with and without pathogenic structural variants. This implies there are no shared facial features in people with diverse underlying genomic abnormalities, which is supported by visual inspection of the average face (Supplementary Fig. 3). FSD may become more widely used as numbers of people with a given pattern of quantitative abnormality (FSD or other construct) increase, and may become of direct clinical use.

Compounding the lack of dysmorphology training in most clinicians caring for people with epilepsy, adult medicine is divided into different specialties, and physicians often do not consider a potential unifying genomic or genetic cause in patients (Maves *et al.*, 2007; Williams, 2007). Being able to recognize and classify facial dysmorphism can lead physicians to consider alternative diagnoses or to request further relevant investigations, and this could be aided by the increasing use of 3D stereophotogrammetry in clinical settings (Heike *et al.*, 2010). MRI abnormalities and intellectual disability are known to correlate with pathogenic structural variants (Hochstenbach *et al.*, 2009; Sagoo *et al.*, 2009; Xiang *et al.*, 2010), as seen in our study population. Any of these observations should prompt detailed genetic studies (Galizia *et al.*, 2012).

Array comparative genomic hybridization is now part of clinical genetics practice, whereas whole exome and genome sequencing are just beginning to make their mark as clinical tests (Johnson *et al.*, 2012; Need *et al.*, 2012). Although in some cases, a clear genetic diagnosis will emerge, in others the mass of data from such tests will need additional interpretation (Hennekam and Biesecker, 2012). Dense surface models could be used for this purpose. We note that whole face FSD was not correlated with the number of genes in the pathogenic structural variant interval when looking at all types of structural variants collectively. People with deletions are, in general, thought to have a more severe phenotype than those with duplications (Hanemaaijer *et al.*, 2012). We found that our patients with deletions had a similar FSD, but a significantly smaller structural variant interval size, by a factor of three to four, than those with duplications. This suggests that for a given interval size, deletions may indeed affect face shape more than duplications. Our findings may seem to be in contrast to a recent study that suggested no difference in duplication length and deletion length in a group of people with epilepsy and pathogenic structural variants (Striano *et al.*, 2012), but this may simply reflect differences in methodology and case numbers. We have only analysed structural variants that were considered pathogenic; facial development is likely to be complex, and in due course, the wider complement of individual genetic variation might be studied using dense surface modelling. Determination of the pathogenicity of structural variants is still an evolving area, and so the contribution of structural variants to phenotypes may be overestimated or underestimated (Craddock *et al.*, 2010; Vermeesch *et al.*, 2011), including those structural variants found in individuals with epilepsy (Striano *et al.*, 2012). Face shape analysis has already been successfully used to help determine the pathogenicity of a novel microdeletion (Hannes *et al.*, 2012), and quantified face shape may help to identify new

syndromes in the new generation of multicentre studies (Firth *et al.*, 2011).

Genes expressed in the forebrain during early development are known to affect human face formation (Marcucio *et al.*, 2011), and we considered the foetal expression of genes contained in the pathogenic structural variants of our patients using public resources. The level of gene expression is a crude measure and does not account for gene interactions or effects of a pathogenic structural variant on genes outside its interval. We found that although whole face FSD was not correlated with the number of genes in a pathogenic structural variant interval, it showed significant positive correlation with the number of contained genes expressed highly in the foetal forebrain (50–200 days). Facial structures develop in late embryonic and early foetal life, driven by complex molecular interactions between surface ectoderm and underlying forebrain and neural crest cells. It is conceivable, therefore, that these forebrain-expressed genes may be candidates for facial development and dysmorphism, and possibly also epilepsy. Also, we noted a trend between a greater number of deleted forebrain-expressed genes and a higher FSD, which needs confirmation in a larger group. It may also be possible to identify individual genes contributing to face shape using dense surface models. A recent genome-wide association study suggests a developmental gene, *PAX3*, may influence the height of the nasal root (Paternoster *et al.*, 2012). *PAX3* is known to be necessary for neural crest cell development and migration, and mutations in *PAX3* are associated with spina bifida and sensorineural hearing loss as well as facial dysmorphism (Pingault *et al.*, 2010). The authors used landmark-based anthropometry, which is less able to detect differences in some facial regions than dense surface modelling (Hammond and Suttie, 2012).

Other related uses for stereophotogrammetry and dense surface models include the further investigation of consequences of structural variants that are already known to be pathogenic. We have used a model previously to show reduced facial fat in a subject with a deletion encompassing a gene involved in fatty acid metabolism (Kasperavičiūtė *et al.*, 2011). The technique may be useful to characterize facial differences in people with novel syndromes, or when pleiotropy is found, such as for 16p13.11 microdeletion.

Our aim was to explore the utility of objective face shape analysis in relation to presence or absence of a known pathogenic structural variant, not in relation to presence or absence of epilepsy itself as a phenotype. We point out that we were not seeking to identify a 'face' associated with epilepsy *per se*. Given the heterogeneity of epilepsy in every aspect, this concept is dangerous nonsense, which we raise specifically to dismiss explicitly. Even in patients with pathogenic structural variants, there were no shared facial features, suggesting actual facial shapes are as varied as the underlying pathogenic structural variants.

There are limitations that need consideration. Landmarking of facial features is the one subjective step in stereophotogrammetry and dense surface modelling. With more experience and optimization of the landmarks used, the intra-operator and inter-operator reproducibility might be further improved as noted in studies using radiographic landmarks (Houston, 1983). In our study, the

operator who landmarked control images was different to the one who landmarked patient images, and a small non-significant reproducibility error was identified. A further potential confounding factor is facial injury. Individuals with epilepsy have a 1.6 times greater risk of accident than the general population (van den Broek and Beghi, 2004), and this is related to the type and frequency of seizures (Tiamkao *et al.*, 2009). Such injuries include fractures, contusions and burns, which often affect the face. Previous facial morphometric studies have ignored facial injuries or excluded such cases on the basis of patients' recall of injuries (Hammond *et al.*, 2005; Evison *et al.*, 2010; Kau *et al.*, 2010). Our findings held after blinded exclusion of cases with suspected acquired facial deformity. The effect of facial expression is less easy to discern. Children and people with intellectual disability may be less likely to maintain a neutral expression during image capture. We used a surrogate marker, lip closure, to determine if expression was neutral in an objective manner; lip closure was associated with differences in FSD and may account for part of the increase in FSD in those with intellectual disability. Point mutations, chromosomal translocations and inversions, and small pathogenic structural variants, with sizes below the threshold for detection by our methods, could also contribute to atypical face shape, and would have been missed. With more comprehensive methods of detecting pathological genetic changes, such as next-generation sequencing techniques, re-evaluation of dense surface models in future datasets will allow further exploration of abnormalities of face shape.

Our findings are in Europeans referred to neurology clinics with a diagnosis of epilepsy. Ethnicity influences facial appearance, and at least in certain genomic disorders, either makes dysmorphic features less obvious or less easily detected by physicians (McDonald-McGinn *et al.*, 2005). We were unable to investigate other ethnicities because of lack of ethnicity matched control subjects for comparison, but we found no difference in the three different groups used here. We found that age had no effect on FSD. This was important to exclude, as it is known that some genetic conditions show greater dysmorphism in childhood, such as Noonan or Beckwith–Wiedemann syndromes (Choufani *et al.*, 2010; Romano *et al.*, 2010).

Anti-epileptic drugs may also be a source of bias in this population. Some drugs, especially 'older' ones (those licensed before ~1990), may have adverse effects on the face, such as gingival hyperplasia, acne, facial coarsening or weight gain (Collaborative Group for Epidemiology of Epilepsy, 1988). The number of drugs and the proportion that took each drug were not significantly different between patients with or without pathogenic structural variants (Supplementary Table 5). Finally, the role of other potential confounding factors, such as body weight, has not been elucidated.

In conclusion, we have shown that 3D stereophotogrammetry and dense surface modelling offer a promising avenue for further evaluation of the full phenotype of epilepsy related to clinically relevant genomic structural variants. We show the technique is robust and reproducible for analysing facial shape. As technical and bioinformatics advances make genomic analysis more comprehensive and available, equal sophistication in phenotyping

methods is likely to prove necessary. Face shape analysis may contribute to deepening phenotypic evaluation.

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## Supplementary material

Supplementary material is available at *Brain* online.

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